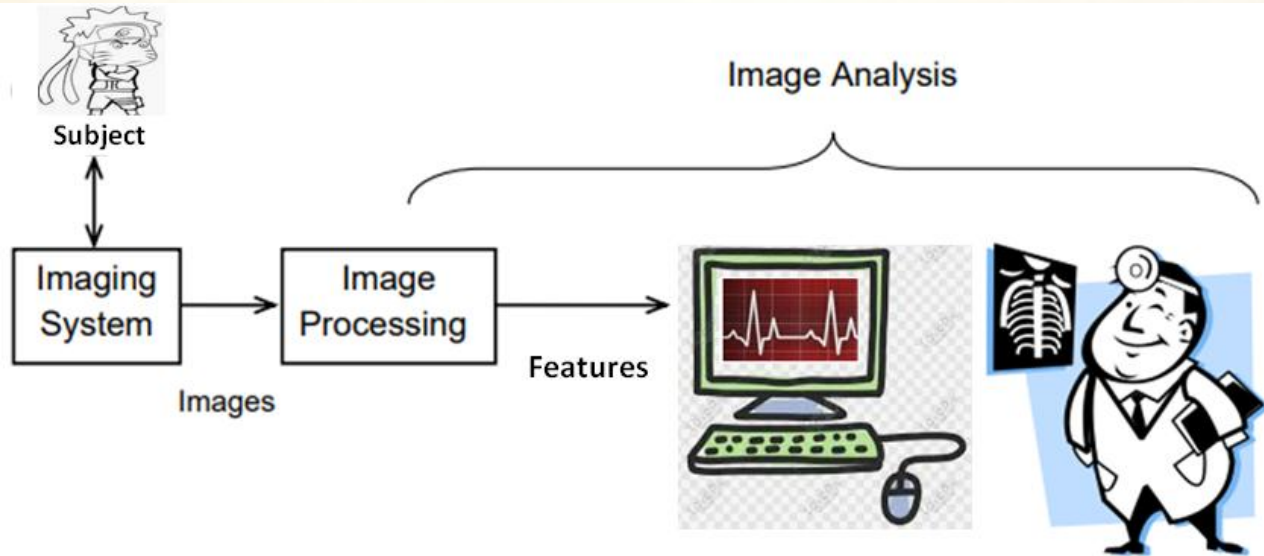


Medical Image Processing

ULTRASOUND TOMOGRAPHY

Introduction

Medical Image Processing



Medical Image Processing

What do images represent?

For medical images, pixels may represent parameters such as:

- X-ray attenuation (density)
- Acoustic impedance (distribution)
- Optical reflectivity (or impedance)
- Electrical activity

Medical Image Processing

Medical images

The values in the image may represent distance, reflectivity, density, temperature, etc.

An image may be composed of:

- 2-D: pixels = picture elements
 - 3-D: voxels = volume elements
 - 4-D and higher: hyper voxels = hyper volume elements
-

Medical Image Processing

Purposes of image processing

- Preprocess image to reduce noise and blur (filtering)
- Identify structures within the image (segmentation)
- Extract “useful” information from the image (quantification, classification)
- Prepare the image for visualization (enhancement, reconstruction)



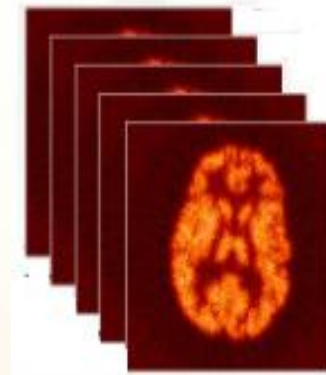
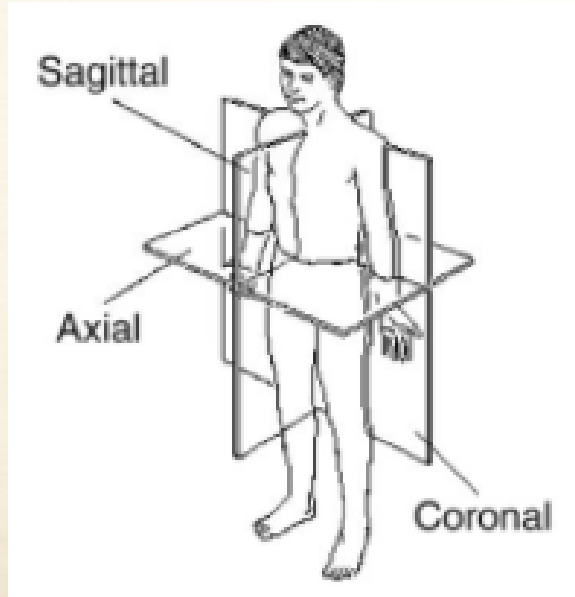
Ultrasound tomography

Tomography

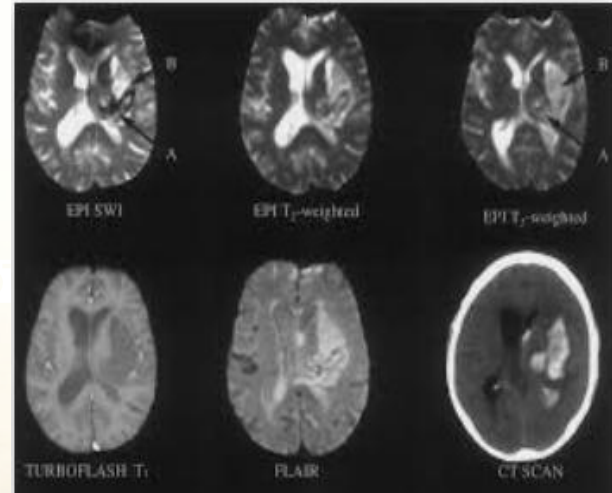
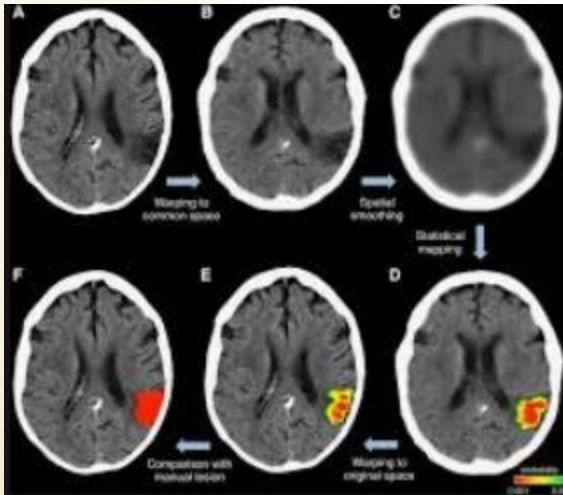
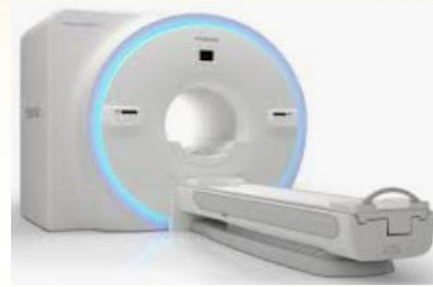
tomos = "slice, section"
graphō = "to write, to describe"



Imaging by sections or sectioning through the use of any kind of penetrating wave



Tomography images



Ultrasound tomography

Ultrasound

Ultrasound uses sound waves to generate a medical image of human anatomy.

The frequency of ultrasound is higher than the sound wave frequencies that can be detected by human hearing.

Sound waves can only travel through a medium, so a water-based gel needs to be applied to the skin, which allows the ultrasound to be transmitted from the transducer or probe into the body.

Ultrasound advantages

- Ultrasound scanning is non-invasive.
- Ultrasound is widely available, easy-to-use and less expensive than other imaging methods.
- Ultrasound imaging uses non ionizing radiation.
- Ultrasound scanning gives a clearer image of soft tissues than x-ray images.
- Ultrasound causes no health problems and may be repeated as often as is necessary.
- There are no hazards for the patient and operator.

Disadvantages :

- Resolution of images is often limited.
- Bone absorbs ultrasound so that brain images are hard to get.
- Attenuation can reduce the resolution of the image.
- Sonography performs very poorly when there is a gas between the transducer and the organ

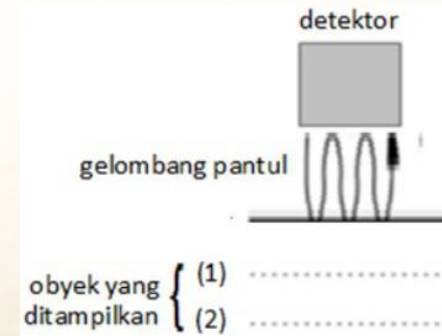
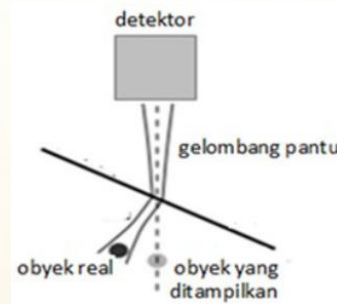
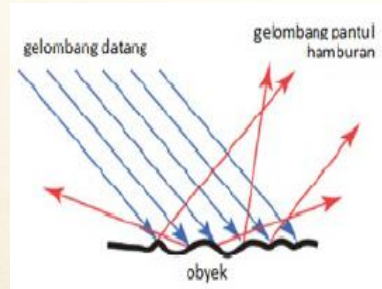
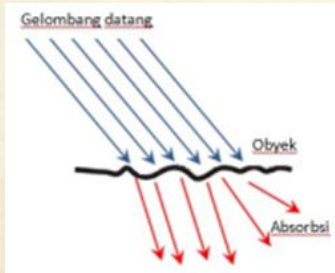
Ultrasound parameters

Medium	Speed of sound (ms ⁻¹)	Characteristic impedance (kgm ² s ⁻¹)	Half depth at 3 MHz (cm)
Blood	1585	1.68 x 10 ⁵	1.2
Liver	1580	1.66 x 10 ⁵	1.7
Muscle skeletal	1575	1.64 x 10 ⁵	1
Fat	1430	1.31 x 10 ⁵	2.5-0.7
Bone (skull)	2800	5.60 x 10 ⁶	0.04
Water (20°C, 1 atm)	1482	1.48 x 10 ⁵	150
Air (20°C, 10% humidity)	331	392	0.2

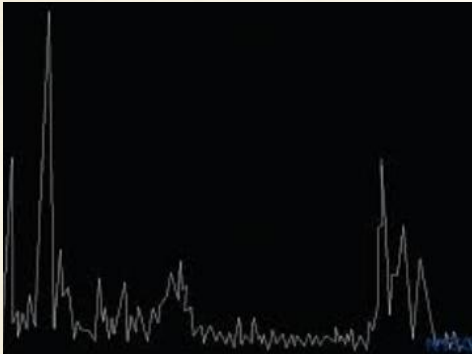
$$v = \sqrt{\frac{C}{\rho}}$$

C is the bulk modulus and ρ is the density of the material

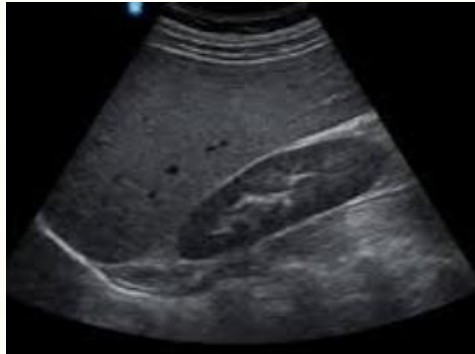
$$s = \frac{t \times c}{2}$$



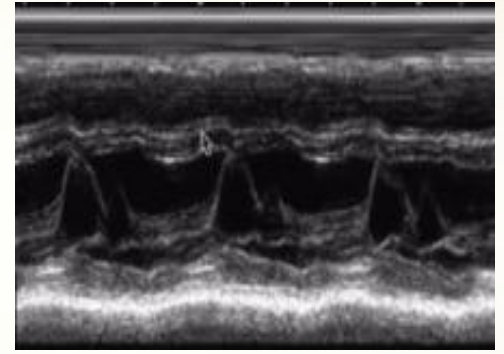
Ultrasound image



A – Mode (Amplitude)
used to judge the depth of an
organ and assess an organ's
dimensions



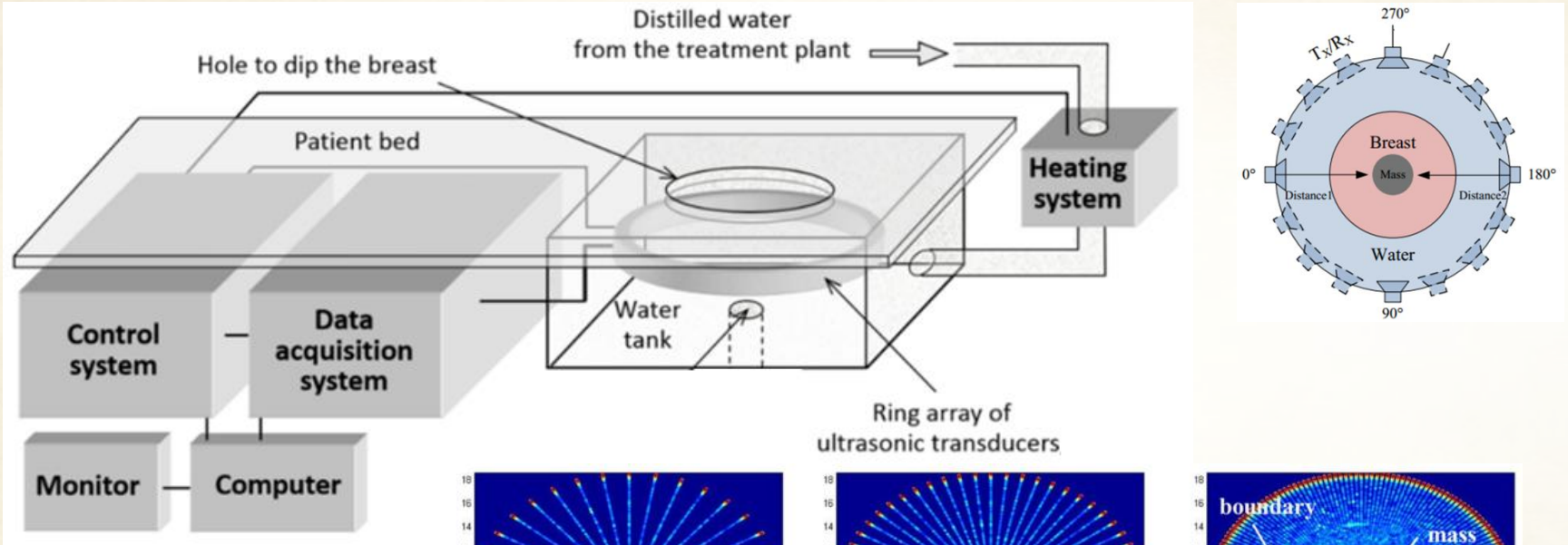
B – Mode (Brightness)
display of a 2D-map of intensity
and most common form of US
imaging



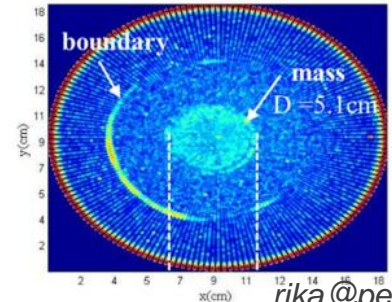
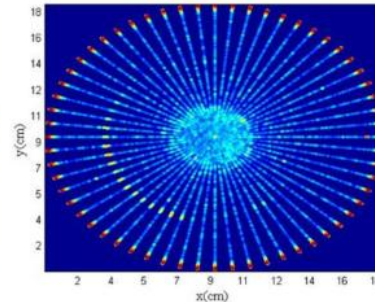
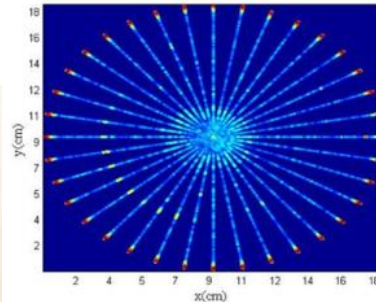
M-mode (Motion)
used for analyzing moving body
parts, commonly in cardiac and
fetal cardiac imaging

Ultrasound tomography

Breast cancer detection – non freehand

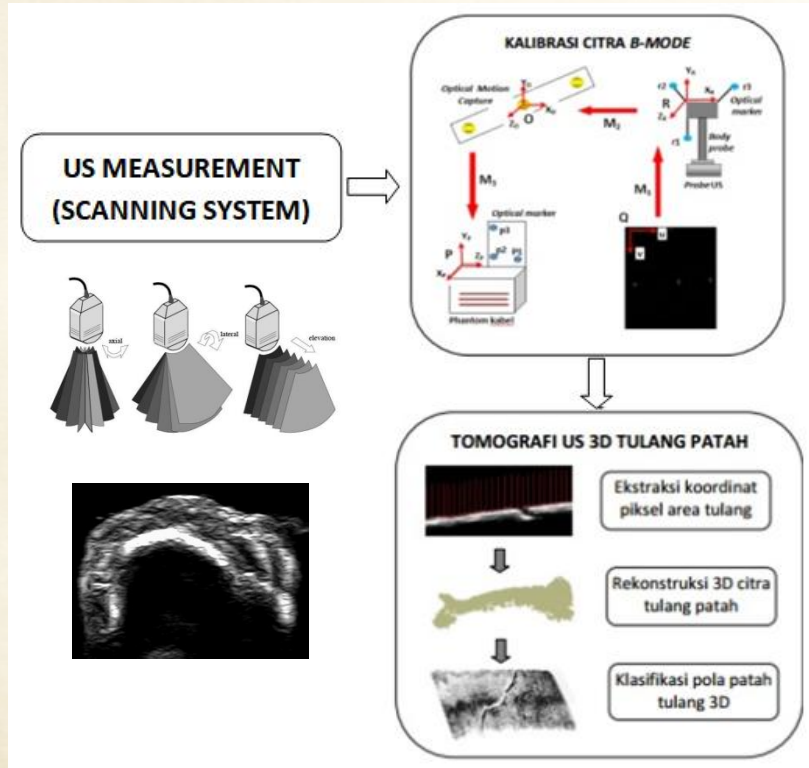


The algorithm only needs to detect the half depth of the detection target



Ultrasound tomography

Long-bone fracture detection -freehand



Freehand : free orientation and position

Calibration using tracker camera and optical marker

Calibration

$$\begin{bmatrix} x \\ y \\ z \\ 1 \end{bmatrix} = M_3 \cdot M_2 \cdot M_1 \cdot S_{xy} \begin{bmatrix} u \\ v \\ 0 \\ 1 \end{bmatrix}$$

$$M_n = \begin{bmatrix} R^R_{(3 \times 3)} & t^R_{(3 \times 1)} \\ \mathbf{0}_{1 \times 3} & 1 \end{bmatrix}$$

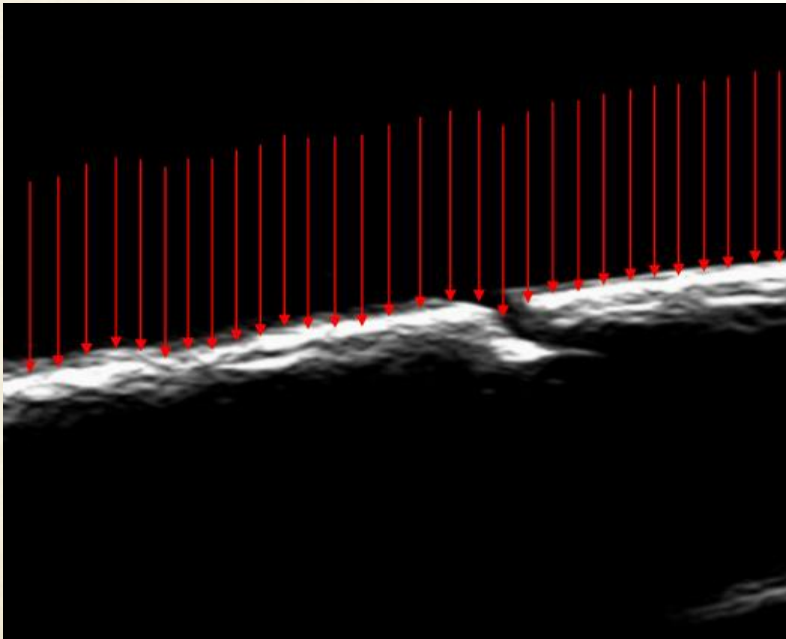
$$R^R = \begin{bmatrix} v_{xR} & v_{yR} & v_{zR} \end{bmatrix}$$

$$t^R = (x_2, y_2, z_2)^T$$

Ultrasound tomography

Pixels coordinate extraction

column scanning \rightarrow edge pixel (u, v)



$$L_i = \begin{bmatrix} u_{i1} & u_{i2} & \cdots & u_{iN_i} \\ v_{i1} & v_{i2} & \cdots & v_{iN_i} \\ 0 & 0 & \cdots & 0 \\ 1 & 1 & \cdots & 1 \end{bmatrix}$$

i = citra B-mode ke - i

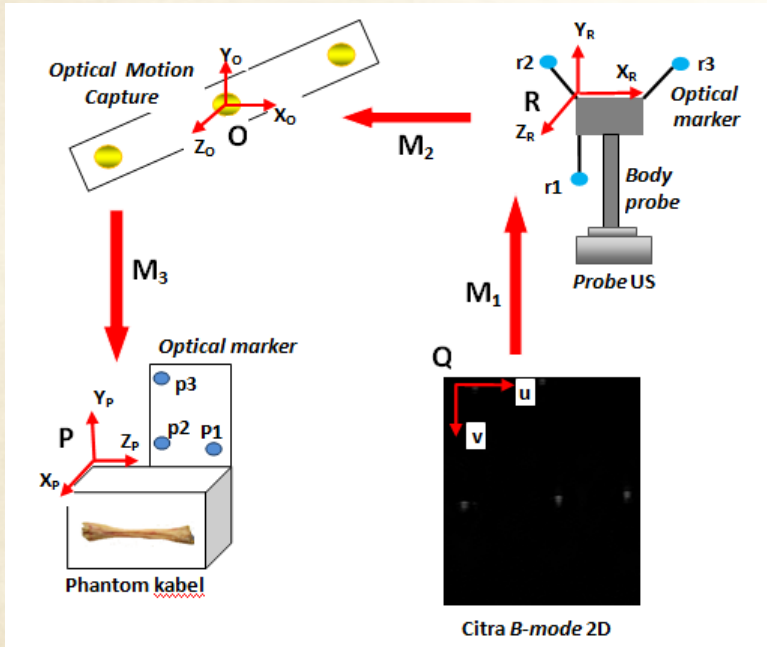
(u, v) = koordinat piksel dalam bidang 2D

N_i = jumlah *edge pixel* dalam citra ke i

N = jumlah citra *B-mode* dalam pemindaian sa
tu obyek tulang

$$l = (l_1, l_2, l_3, \cdots, l_N)$$

Ultrasound tomography



$$Q = (Q_1, Q_2, Q_3, \dots, Q_N)$$

$$Q_i = M_{3i} \cdot M_{2i} \cdot M_1 \cdot S_{xy} \cdot L_i$$

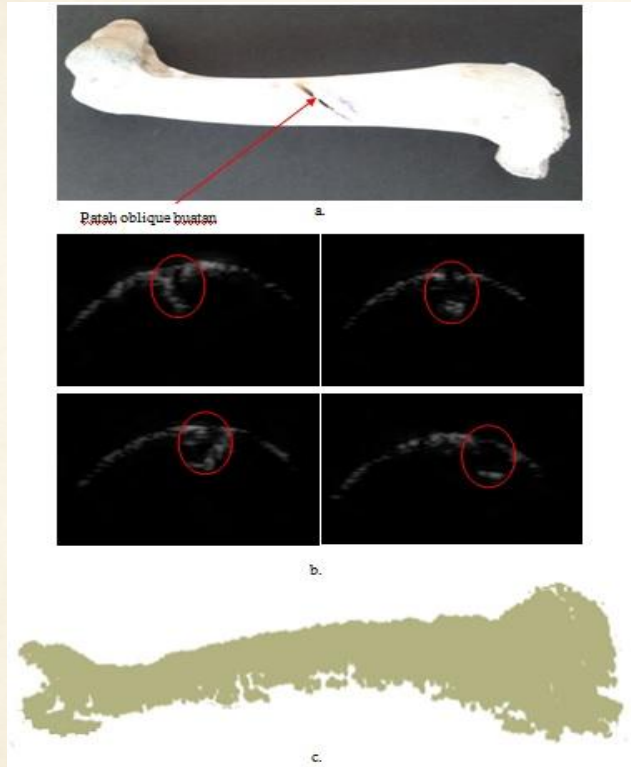
$$L_i = \begin{bmatrix} u_{i1} & u_{i2} & \dots & u_{iNi} \\ v_{i1} & v_{i2} & \dots & v_{iNi} \\ 0 & 0 & \dots & 0 \\ 1 & 1 & \dots & 1 \end{bmatrix}$$

$$S_{xy} = \begin{bmatrix} 0.0804 & 0 & 0 & 0 \\ 0 & 0.0804 & 0 & 0 \\ 0 & 0 & 1 & 0 \\ 0 & 0 & 0 & 1 \end{bmatrix}$$

$$A_i = \begin{bmatrix} a_{i11} & a_{i12} & a_{i13} & a_{i14} \\ a_{i21} & a_{i22} & a_{i23} & a_{i24} \\ a_{i31} & a_{i32} & a_{i33} & a_{i34} \\ 0 & 0 & 0 & 1 \end{bmatrix}$$

$$M_1 = \begin{bmatrix} m_{11} & m_{12} & m_{13} & m_{14} \\ m_{21} & m_{22} & m_{23} & m_{24} \\ m_{31} & m_{32} & m_{33} & m_{34} \\ 0 & 0 & 0 & 1 \end{bmatrix}$$

Ultrasound tomography



Tulang kambing : jarak antar slice
min 0.3084



Sekian terima kasih...